# Effect of channel width on droplet generation inside T-junction microchannel

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#### ABSTRACT

In a T-junction microchannel, channel geometry plays a major role that affects the physics behind droplet generation. The effect of channel width on droplet size and frequency in a T-junction microchannel is investigated in the present study. The current work is an extension of our previous work, where a model was developed to predict the size of the droplets generated in a T-junction microchannel when both the continuous and dispersed phase channels have equal widths. In the present work, we extended the model to account for the varying width ratio between the dispersed and continuous phase channels. We performed in-house experiments by varying the channel width and viscosity ratios between the fluids to study the size of the droplets generated and to validate the proposed scaling law. We further investigated the effect of channel geometry on the frequency of droplet generation in the T-junction microchannels. The experimental results show that the droplet length increases with an increase in the width of the continuous phase channel. With variations in the width of the dispersed phase channel, similar behavior in droplet sizes and the frequency of droplet production is observed. The analysis of this study provides new insight into the effect of channel width on the droplet length and frequency. Overall, this research intends to provide a thorough understanding of the design of microchannels based on the geometry and manipulation of droplets with varying widths.

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#### I. INTRODUCTION

Nowadays droplet-based technology provides a wide range of platforms for producing micro- and nanodroplet in a channel having a cross section in the order of a micrometer. Because of precise and controlled droplet generation, the faster reaction inside the microchannel, and interdisciplinary applications, it has attracted remarkable attention over the past 20 years. Apart from fundamental and technical aspects, droplet microfluidics has many broad areas of applications such as drug delivery,<sup>1,2</sup> biology,<sup>3-5</sup> clinical diagnostics,<sup>6</sup> materials science,<sup>7</sup> and emulsions in food<sup>8</sup> and textile industries. Droplet microfluidics serves as the foundation for cell encapsulation and digital polymerase chain reaction, which enables single cell analysis and quick diagnosis of a variety of diseases. Using this method, water in oil (W/O), oil in water (O/W), and gas-liquid droplet generation in microchannel having a particular size and pattern is possible. The advantages of droplet microfluidics include simple and resilient droplet generation, superior handling, production of monodisperse droplets, and precise droplet control. The produced droplets can be controlled independently with increased throughput, scalability, and substantial consistency.9

To date, microchannels having rectangular-, square-,<sup>10</sup> circular-,<sup>11</sup> and U-shaped<sup>12</sup> cross sections have been investigated. The rapid advancement of microfabrication technology permits droplet microfluidics for enhanced control over diverse fluid interface interactions and manipulation of discrete droplets within microchannels. To generate homogeneous droplets inside a microchannel, many microfluidic techniques such as co-flow,<sup>13–15</sup> T-junction,<sup>16–19</sup> and flow-focusing<sup>20–22</sup> have been put forward. Due to monodispersed droplet formation, simplicity in design, ease of manufacturing, and faster reactions inside a microchannel, T-junction is extensively used for droplet generations.<sup>16–18,23–25</sup> Recently, researchers have modified the T-junction with a contractive structure<sup>26–28</sup> and a step structure<sup>29</sup> and initiated a study into the physics underlying droplet dynamics. Both active<sup>30,31</sup> and passive techniques<sup>32</sup> were used for the generation of droplets. T-junction is a passive method of droplet generation, in which the monodispersed droplets with uniform spacing between the droplets are generated. The current work focuses on the T-junction having a rectangular cross section.

Thorsen *et al.*<sup>16</sup> first reported the formation of aqueous droplets in oil in a T-junction using pressure-controlled flow. They explained

the dynamics of droplet size generation in terms of tangential shear stresses and interfacial forces. Later, several studies<sup>17,18,33–37</sup> were carried out to understand the effect of different parameters. The factors responsible for the droplet formation within a T-junction are geometrical parameters such as channel width, flow properties such as the flow rate of the continuous and dispersed phases, pressures at the inlet of the channel, fluid properties such as viscosity,<sup>38,39</sup> interfacial tension, and wetting properties such as contact angle.<sup>40</sup> The effect of these properties can be formulated as the non-dimensional numbers, such as the capillary number of the continuous phase (*Ca<sub>c</sub>*), the Weber number of the dispersed phase (*We<sub>d</sub>*), the flow rate ratio between the dispersed phase fluid and the continuous phase fluid ( $\phi$ ), and the widths of the dispersed phase channel to the continuous phase channel ( $w_d/w_c$ ).

Three important regimes, namely, the squeezing regime that occurs at low Ca<sub>c</sub>, the dripping regime at moderate Ca<sub>c</sub>, and the jetting regime at high Ca<sub>c</sub>, were extensively investigated. Researchers found that the size of the droplets generated in squeezing and dripping regimes can be controlled and, thus, termed the regimes as stable. However, the jetting regime is accompanied by instabilities along the flow, which complicate the task of controlling droplet sizes.<sup>4</sup> Christopher et al.<sup>42</sup> investigated the effect of capillary number, flow rate ratio, channel geometry, and viscosity ratio for droplet breakup in the T-junction. They varied the dispersed phase channel width  $(w_d)$ while maintaining the constant depth (h) and the width of the continuous phase channel  $(w_c)$ . The same group observed that the droplet volume is nearly constant for width ratio  $(w_d/w_c)$  less than one and increases linearly for ratios greater than one for different capillary numbers, and is highly responsive to width ratio for low  $Ca_c$ . Droplet generation rate using T-channel first proclaimed by Nisisako group.<sup>13</sup> Their group discovered that frequency increases linearly with an increase in continuous phase velocity. Later, Christopher and co-workers<sup>42</sup> showed that the droplet formation frequency increases with capillary number but is inversely related to droplet volume. They argued that the frequency increases linearly at low Ca, followed by a power-law behavior ( $f \propto Ca^{4/3}$ ) at higher *Ca*. Wehking *et al.*<sup>43</sup> experimentally studied the effect of channel geometry on droplet generation and frequency by varying the aspect ratio  $(h/w_c)$  while maintaining h constant, where h is the channel height and  $w_c$  is the width of the continuous phase channel. They found that droplet volume decreases and production rate increases as the aspect ratio increases. Though many scaling laws were developed for the droplet size, appropriate physics is still lacking, when both the channel widths are varying. Recently, Jena et al.<sup>37</sup> developed an extensive model for predicting droplet length with uniform channel width for both the continuous and dispersed phase fluid. The developed model works very well for both the squeezing and dripping regimes. Along with the three major forces pressure force, shear force, and interfacial tension, the developed model includes the inertial force of the dispersed phase for droplet breakup and predicts the droplet size.

In the current work, we carried out experiments on T-junction microchannels having continuous phase channel widths ( $w_c$ ) of 250, 280, 350, and 440  $\mu$ m and dispersed phase channel widths ( $w_d$ ) of 250, 360, and 460  $\mu$ m. Fluid combinations having different viscosity ratios  $\lambda = \mu_d/\mu_c$  were chosen. During the experiments, the capillary number of the continuous phase ( $Ca_c$ ), and the flow rate ratios ( $\phi$ ) were varied. In continuation of our previous work,<sup>37</sup> we formulated an analytical

model for the droplet size. The novelty of the present work is that, at a wide range of  $w_c$ , and  $w_d$ , we can predict the droplet size in both squeezing and dripping regimes. In our previous work, we established a model that functions effectively when the widths of both channels are identical. However, the model does not study the effect of channel widths on the breakup of the droplets. Though the effect of flow properties was established in our prior work, the current model demonstrates its robustness by forecasting the droplet lengths for the varying geometrical properties. The merging of the curves, irrespective of flow rate and channel width for a particular fluid, shows its potential in manipulating droplets inside the microchannel. A constant slope of 0.4 is seen for various continuous-phase fluids, demonstrating that the model can predict the droplet size for varying flow properties and geometrical properties.

#### II. MODEL FOR THE DROPLET SIZE HAVING DIFFERENT CONTINUOUS PHASE CHANNEL WIDTH

Droplet generation in a microfluidic T-junction occurs due to the competition of different forces between the continuous phase fluid and the dispersed phase fluid flowing through the channel. Figure 1 depicts a three-dimensional view of the T-junction as well as channels with variable widths.  $w_c$  and  $w_d$  are the inlet channel widths, and h is the depth of the channel, where subscripts c and d stand for continuous and dispersed phases. Continuous phase fluid (oil) flows through the main channel, and the side channel is used for the transport of dispersed phase fluid (DIW). When the two liquids meet at the junction, an interface is created, which grows depending on the forces acting on it. After some time, necking takes place at the junction's interface, which continues to become narrow as the flow continues and droplet



**FIG. 1.** (a) Three-dimensional view of microfluidic T-junction. (b) Configuration of different channel geometry used for conducting the experiment. For all channels, h is taken as  $200 \,\mu$ m.

breakup takes place. The formation of droplets inside the microchannel is influenced by a number of factors, including the geometry of the channel, the flow rate, and the viscosity of the fluid, among others. The current investigation focuses on the analytical modeling of the droplet size by modifying our previous model. The model includes the effect of different continuous phase channel widths on droplet generation. The primary forces studied are the pressure difference at the upstream and downstream edges of the droplet  $(F_p)$ , shear forces from the continuous phase  $(F_{\tau})$ , force due to interfacial tension  $(F_{\sigma})$ , and the dispersed phase inertia force. The summary of the abbreviations is included in the nomenclature of the supplementary material.

Using Newton's second law of motion suggests that the rate of change of momentum of a control mass accounts for the net force acting on it. A schematic of the control mass of the droplet with other variables is shown in Fig. 2. Referring to our previous work,<sup>37</sup> when a detachment of droplet happened, we could write,  $d(mu)/dt = \sum F_{external}$ .

$$F_{\tau} + F_p - F_{\sigma} = m \frac{du}{dt} + u \frac{dm}{dt}, \qquad (1)$$

where *m* and *u* are the mass and velocity of the control mass, respectively. The pressure force  $(F_p)$  and shear force  $(F_\tau)$  act to deform the droplet, and the force due to interfacial tension  $(F_\sigma)$  resists the deformation of the droplet. When the gap between the droplet interface and the top wall of the channel  $(w_g)$  is very small as compared to  $w_c$ , the pressure force is estimated using lubrication analysis as  $F_p = \Delta p w_c h \sim O(\mu Q_c w_c L/w_g^3)$ . The shear force and force due to interfacial tension are estimated as  $F_\tau = \tau w_c h \sim O(\mu Q_c L/w_g^2)$  and  $F_\sigma \sim \sigma h$ , respectively. Using these forces and expanding  $Q_c$ , the analytical model is developed for varying  $w_c$  and  $w_d$ . By considering the above three forces from Garstecki *et al.*,<sup>17</sup> the modified equation can be written as

$$\mu_c U_c L\left(\frac{w_c}{w_g^2}\right) h + \mu_c U_c L\left(\frac{w_c^2}{w_g^3}\right) h \sim \sigma h + \rho_d U_d w_d h u.$$
(2)

The length of the droplet *L* in Eq. (2) will be non-dimensionalized by using the length scale  $l_s$  which is taken as  $w_d$  for the channels with varying continuous phase channel width and as  $w_c$  when the dispersed phase channel width is varied. The velocity *u* in the last term of the Eq. (2) is scaled as the average of the continuous phase and the



dispersed phase velocities (i.e.,  $u \sim (U_c + U_d)/2$ . By applying the above-mentioned scaling to the equation and dividing throughout with  $\sigma h$ , the equation can be rewritten as

$$Ca_{c}\frac{L}{l_{s}}\left(\frac{w_{c}l_{s}}{w_{g}^{2}}\right) + Ca_{c}\frac{L}{l_{s}}\left(\frac{w_{c}l_{s}}{w_{g}^{3}}\right) \sim 1 + We_{d}\left(\frac{\frac{w_{d}}{w_{c}} + \phi}{2\phi}\right).$$
(3)

Here,  $We_d$  is the dispersed phase Weber number, and  $Ca_c$  is the continuous phase capillary number. Equation (3) implies that the forces from the continuous phases that try to break up the dispersed phase thread are balanced by the dispersed phase inertial forces that prevent the thinning of the dispersed phase neck. Equation (3) can be represented as follows:

$$\frac{L}{l_s} Ca_c f\left(\frac{w_c l_s}{w_g}\right) \sim 1 + We_d\left(\frac{w_d}{w_c} + \phi\right). \tag{4}$$

The scaling model presented in the manuscript considers all the important forces responsible for droplet breakup inside a T-junction microchannel. The proposed model works well for both the continuous phase and dispersed phase channel widths for predicting droplet length which is not addressed until now.

#### **III. EXPERIMENTAL PROCEDURE**

A wide range of experiments was conducted for varying continuous phase channel width by using silicone oil and hexadecane oil as continuous phase fluids (Sigma Aldrich). Distilled water (DIW) was taken as the dispersed phase in all cases. The fluids are Newtonian in nature. The continuous phase fluids were selected to show the effect of viscosity variations. The physical properties of the fluids and flow parameters that varied in the experiments are given in Table I. The viscosity was measured using a rheometer (cone and plate type, Anton Paar) and an Oswald viscometer (U-tube type). The pendant drop method<sup>44</sup> was used for interfacial tension measurement with an accuracy of 98%. Computer numerical control (CNC) micro milling (The Cool Tool®) and thermal bonding techniques were employed to manufacture the different microchannels. The thermal bonding technique is used to seal the two sheets of polymethyl methacrylate (PMMA) for 45 min, and then the channel is allowed to cool for 30–45 min. A 200  $\mu$ m diameter end mill tool is used for preparing the microchannel on a (PMMA) sheet of dimension  $50 \times 30 \times 5 \text{ mm}^3$ . Different continuous phase channel widths having dimensions of 250, 280, 350, and 440  $\mu$ m were fabricated. The channels with varying  $w_c$ have a uniform dispersed phase width of  $250 \,\mu\text{m}$ . Also, channels with varying dispersed phase widths ( $w_d = 250$ , 360, and 460  $\mu$ m) are

**TABLE I.** The physical properties of two continuous phase fluids are specified here. For dispersed phase fluid, distilled water (DIW) is taken for conducting experiments. The dynamic viscosity and density of DIW are  $\mu_d = 0.99 \,\mathrm{mPa}\,\mathrm{s}$ , and  $\rho_d = 1000 \,\mathrm{kg/m^3}$ , respectively.

| Continuous<br>phase | $\rho ~(\mathrm{kg/m^3})$ | $\phi$             | λ      | $\sigma$ (mN/m) |
|---------------------|---------------------------|--------------------|--------|-----------------|
| Hexadecane          | 773                       | 0.25, 0.5, and 1.0 | 0.4167 | 37.68           |
| Silicone oil        | 960                       | 0.25, 0.5, and 1.0 | 0.0146 | 48.15           |

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FIG. 3. The in-house experimental set up developed for generating droplets inside microfluidic T-junction is shown here. The channel has two inlets and one outlet. The cross section of the channel is rectangular.

prepared. All the channels have a uniform depth of 200  $\mu$ m. Initially, the channel was hydrophilic in nature and converted to hydrophobic with the chemical treatment of aquapel solution (Pittsburgh Glass Works LLC, USA). To inject the fluids through the microfluidic Tjunction, a dual-channel syringe pump (Holmarc Inc.) was used. First, priming is carried out by flowing continuous phase liquid through the main channel, and then dispersed phase fluid is injected from the side channel to generate droplets. For visualizing the droplet production process, an inverted microscope (Olympus, Japan) was used. A highspeed camera (Photron FASTCAM mini UX) was used to record the experimental occurrence of droplet generation at 10000 frames per second with a resolution of  $1280 \times 480$  pixels. Then, post-processing of the video was accomplished frame by frame to quantify the parameters. The image processing and data analysis of the experimental results were carried out using the Photron FASATCAM viewer and ImageJ software. The high-speed camera's built-in Photron FASTCAM Viewer software is utilized for measuring the length of the droplet during the post-processing of the images. We calibrate the software to our specifications prior to measuring the image. Our measurements involve an objective lens with a 4× magnification and images recorded at a rate of 10 000 frames per second. We used a glass slide calibrator to obtain the relationship between the pixels and the physical lengths in micrometer. In our case, it is  $2.54 \,\mu$ m/pixel. All the experiments were performed at room temperature (about 25 °C). The observations were taken once the device reached a steady state after setting the flow rates for each phase. Each experiment was conducted three times, and  $L/w_d$  is taken as the average of the individual experimental runs. The assembled in-house experimental setup is shown in Fig. 3.

#### IV. RESULTS AND DISCUSSION

Water droplets in oil were generated by injecting oil (continuous phase fluid) in the main channel and DIW (dispersed phase fluid) in the side channel. To acknowledge the effect of different  $w_c$  on droplet generation, the experimental results are plotted in Fig. 4. Three distinct regimes, i.e., squeezing, dripping, and jetting, are found during the droplet formations in all three continuous phase channel widths.

However, the transition point from squeezing to dripping and dripping to jetting decreases as  $w_c$  increases.

The length of the droplet decreases with an increase in the continuous phase capillary number, which follows a similar trend for all the three continuous phase channel widths as shown in Fig. 4. It is also observed from the experiments that with an increase in  $w_c$ , the droplet length increases for both fluid combinations. The possible reason could be that as  $w_c$  increases, the flow rate of continuous phase fluid increases, which imposes a larger inertia force on the protruding interface. For the same  $Ca_c$ , the increased  $w_c$  drags the interface to a larger length before droplet breakup occurs. It was previously found that when  $Ca_c$  increases, the droplet length decreases. Hence, the gap



**FIG. 4.**  $L/w_d$  is plotted against the  $Ca_c$  for  $w_c = 250$ , 280, 350, and 440  $\mu$ m for hexadecane and silicone oil as continuous phase fluid for different  $\phi$ . The non-dimensional droplet length  $L/w_d$  decreases with an increasing capillary number  $Ca_c$  and increases with an increase in  $w_c$  and  $\phi$ .

between the interface of the droplet and the main channel wall  $(w_g)$  increases. For varying  $w_c$ , it was noticed from our experimental findings that  $w_g$  increases with an increase in  $w_c$ , which is in accordance with the model shown in Eq. (4).

For a constant  $Ca_c$ , the results are shown in Fig. S1 in the supplementary material, along with the corresponding experimental images in Fig. S2. Moreover, it can be observed from our model that the ratio of  $w_c/w_g$  inversely affects  $Ca_c$ . Our in-house experimental results show the same phenomena for different  $w_c$  and fluid combinations. In another set of experiments, we vary dispersed phase channel width  $(w_d)$ . When  $w_d$  varies from 250 to 460  $\mu$ m, the droplet length increases. When  $w_d$  increases, the velocity of the dispersed phase decreases. As a result, the movement of the interface becomes shorter, which will slow down the penetration. Before breaking up, the interface expands to a greater length, and the droplet's length continues to grow. Experiments are conducted by using silicone oil as a continuous phase fluid for flow rate ratios of 0.5 and 1. The non-dimensional droplet length is taken as  $L/w_c$  and the results are depicted in Fig. 5. The experimental results presented in the manuscript are conducted three times for each data point and the average of the data are taken. The maximum uncertainty in the measurement of length is  $\pm 0.05$  and for frequency, it is  $\pm 0.06$ .

Equation (4) suggests that  $w_g$  is directly proportional to both  $w_c$ and  $Ca_c$ . From Fig. S1, it is observed that the slope of  $w_g/w_c$  is nearly constant at low  $Ca_c$ , which increases with an increase in  $Ca_c$ . At a constant  $Ca_c$ , as  $w_c$  increases, the change in slope is greater, which occurred due to the increase in the flow rate of the continuous phase. When  $w_c$  is larger, the shear force tends to dominate, which causes the interface to become narrower before it blocks the main channel. This results in an increase in  $w_g$  for a given  $Ca_c$ . Based on the findings of the study, it can be concluded that  $w_g$  is more responsive toward  $w_c$  at



**FIG. 5.**  $L/w_c$  is plotted against the  $Ca_c$  for  $w_d = 250$ , 360, and 460  $\mu$ m for silicone oil as continuous phase fluid for different  $\phi$ . The non-dimensional droplet length  $L/w_c$  decreases with an increasing capillary number  $Ca_c$  and increases with an increase in  $w_d$  and  $\phi$ .



**FIG. 6.** Experimental images illustrating droplet length and  $w_g$  for  $w_c$ : (a) 250, (b) 350, and (c) 440  $\mu$ m for a constant  $We_d$ . It was noticed that  $w_g$  increases from 137 to 199  $\mu$ m as  $w_c$  increases from 250 to 440  $\mu$ m. The results shown here are for silicone oil as a continuous phase fluid with a flow rate ratio  $\phi = 0.5$ .

higher  $Ca_c$ . Our experimental findings further imply that, for a fixed  $We_d$ , both the droplet length and  $w_g$  increase with an increase in continuous phase channel widths (Fig. 6). At constant  $We_d$ , the inertia force of the dispersed phase, which opposes the neck from becoming narrow, is constant. However, due to an increase in  $w_c$ , the pressure exerted by the continuous phase liquid on the dispersed phase fluid increases. Due to this, the dispersed phase liquid will take a longer time to build up sufficient pressure to penetrate the massive volume of the main channel. Our experimental findings demonstrate that for a fixed  $Ca_c$ , the time between penetration of interface till necking  $(t_{PN})$ increases. As  $w_c$  increases, the increase in  $t_{PN}$  delays the interface to move along the flow. As a consequence of this, the interface is pulled to a greater length prior to the occurrence of droplet breakup, which contributes to an increase in droplet length. For a particular  $Ca_c$ , the  $t_{PN}$  for different  $w_c$  is shown in Fig. 7. When there is an increase in  $w_d$ , the dispersed phase velocity decreases, which results in an increase in  $t_{PN}$ . Because of this, the length of the droplet before it disintegrates is increased.

In our previous work, scaling was accomplished by taking results for a constant  $w_c$ . Considering our former model as a reference, we plot the results for different  $w_c$  by taking  $L/w_c$  as non-dimensional



**FIG. 7.** Experimental images showing  $t_{PN}$  for  $w_c = 250$ , 350, and 440  $\mu$ m for a constant  $Ca_c$ . It was observed that  $t_{PN}$  increases as  $w_c$  increases from 250 to 440  $\mu$ m. The results are for silicone oil taken as a continuous phase liquid. All the results plotted here are for  $Ca_c = 5.02 \times 10^{-2}$ .

droplet length. For different  $w_c$ , the results are aligned in a parallel fashion to each other, as shown in Fig. 8. However, by altering the model by taking  $L/w_d$  as the dimensionless droplet length, we were able to see a single merged curve for a specific viscosity ratio.

From Eq. (4), it can be observed that for varying  $w_c$ , the nondimensional droplet length  $L/w_d$  along with  $Ca_c$  depend on both  $We_d$ and  $w_c$ .  $We_d$  can be explained in terms of the inertia force of the dispersed phase, which counters the squeezing of the neck at the junction of the microchannel. Therefore, in Fig. 9, the plot displays  $L/w_d \times Ca_c$ 



**FIG. 8.**  $L/w_c \times Ca_c$  is plotted against the  $We_d(\frac{\frac{m}{2}+\phi}{2\phi})$  on a log-log scale for different  $w_c$ ,  $\lambda$ , and  $\phi$ . The slope of the y-axis with respect to the x-axis is found to be 0.4.



**FIG. 9.**  $L/w_d \times Ca_c$  is plotted against the  $W_{ed}(\frac{\frac{w_c}{2} + \phi}{2\phi})$  on a log-log scale for different  $w_c$ ,  $\lambda$ , and  $\phi$ . The slope of the y-axis relative to the x-axis is found to be 0.4. For three different  $w_c$ , it is observed that the experimental results coalesce into a single curve for a particular fluid combination.

on vertical axis, whereas  $We_d [(w_d/w_c) + \phi]/2\phi$  is displayed on the horizontal axis. As  $w_c$  increases, the shear force becomes more dominant over interfacial tension. The continuous phase exerts a significant amount of shear force that tries to squeeze the neck of the interface and drag it to move parallel with the flow. At the same time, the effect of the inertia force of the dispersed phase plays an important role in droplet breakup. The dispersed phase inertia force offers resistance in terms of dynamic pressure to the squeezing of the neck.<sup>37</sup> As the value of  $w_c$  increases from 250 to 440  $\mu$ m, the droplet length increases due to the combined effects of  $w_c$  and the inertial force that results from the dispersed phase. We have performed statistical analysis for three aspect ratios  $(h/w_c)$  with a confidence level of 95%. The aspect ratios are 0.8 ( $w_c = 250 \,\mu\text{m}$ ), 0.571( $w_c = 350 \,\mu\text{m}$ ), and 0.454( $w_c = 440 \,\mu\text{m}$ ) when silicone oil is utilized as the continuous phase. The aspect ratios for hexadecane oil as a continuous phase are 0.714 ( $w_c = 280 \,\mu\text{m}$ ),  $0.571(w_c = 350 \,\mu\text{m})$ , and  $0.454(w_c = 350 \,\mu\text{m})$ . For all cases, the depth of the channel is maintained as  $200 \,\mu\text{m}$ . With a confidence level of 95%, the droplet length can be predicted for different aspect ratio microchannels for silicone oil ( $Ca_c = 0.0012-0.22$ ) and hexadecane  $(Ca_{c} = 0.00015 - 0.02)$ , as indicated in the Figs. S4 and S5 in the supplementary material.

Additionally, we carried out studies by altering  $w_d$  taking silicone oil as the continuous phase. When  $w_d$  varies by plotting  $L/w_d \times Ca_c$ against  $We_d [(w_d/w_c) + \phi]/2\phi$ , the results lay parallel to each other as shown in Fig. 10. The results are quite similar when  $w_c$  varies. By observing the results from varying  $w_c$ , for different  $w_d$ , we change the non-dimensional droplet length to  $L/w_c$  as  $w_c$  is constant. Then,  $L/w_c \times Ca_c$  for different  $w_d$  is mapped against  $We_d [(w_d/w_c) + \phi]/2\phi$ . It is found that the curves merge to a single curve for different  $w_d$ . The results are shown in Fig. 11. From the plot, it can be observed that  $L/w_c \times Ca_c$  increases with an increase in  $We_d [(w_d/w_c) + \phi]/2\phi$  up to a certain point, beyond which there is a change in the slope. This shift



**FIG. 10.**  $L/w_d \times Ca_c$  is plotted against the  $We_d(\frac{w_d + \phi}{v_d \phi})$  on a log –log scale for different  $w_c$ ,  $\lambda$ , and  $\phi$ . The slope of y-axis with respect to x-axis is found to be 0.4.

in slope suggests a transition from dripping to the jetting regime. For a specific viscosity ratio, it can be noticed from Fig. 11 that all the data collapse to a single curve, irrespective of dispersed phase channel widths and flow rate ratios. The above discussion leads us to the conclusion that channel width has a profound effect on droplet formation. It is possible to obtain a single merged curve for a given viscosity ratio when both the channel widths are varied while keeping other variables constant. From the model, we can predict the droplet size with respect to  $Ca_c$  by knowing the flow rate ratio ( $\phi$ ) and Weber number of the dispersed phase ( $We_d$ ). Regardless of the flow rate ratios for a

particular continuous phase fluid, the data are merged into a single curve, as depicted in Figs. 9 and 11. A constant slope of 0.4 is seen for various continuous-phase fluids, demonstrating that the model can predict the droplet size when both channel widths vary.

In addition to the droplet size, droplet production frequency is another important parameter that is addressed here. In the current work, the frequency of droplet generation is also analyzed. The frequency of droplet production depends upon the flow rate ratio, capillary number of the continuous phase, channel dimensions, and Weber number of the dispersed phase. Droplet production rates are calculated for three different continuous phase channel widths for varying flow rate ratios and fluid combinations. Based on the experimental footage, an estimate of the droplet formation rate per unit interval of time was developed. It is observed that the frequency increases with an increase in flow rate ratio but decreases with continuous phase channel width. In the research that has been provided, the flow rate ratio is altered by changing the flow rate of the dispersed phase while maintaining the constant flow rate of the continuous phase. As the flow rate ratio increases, the time it takes for the dispersed phase fluid to penetrate decreases. The shear force from the continuous phase breaks the interface quickly, which results in a faster formation rate. However, for a particular capillary number, with an increase in  $w_c$ , it offers higher resistance to penetration, which decreases the frequency generation rate. The results for frequency of droplet generation (f) concerning the capillary number of the continuous phase are plotted in Fig. 12 for different continuous phase channel widths. It is also observed that frequency increases slowly at low  $Ca_c$  but rapidly at higher  $Ca_c$ .

It is also noticed that for a fixed  $Ca_c$ , the production rate decreases with an increase in continuous phase channel width ( $w_c$ ). The findings for different  $Ca_c$  are plotted and shown in Fig. S3. A similar behavior in the frequency of droplet generation is observed for the varying dispersed phase channel widths ( $w_d$ ). The length of the droplet is observed to increase with an increase in the dispersed phase channel



**FIG. 11.**  $L/w_c \times Ca_c$  is plotted against the  $We_d(\frac{w_d + \phi}{2\phi})$  on a log –log scale for different  $w_c$ ,  $\lambda$ , and  $\phi$ . It is observed that the experimental results merge to a single curve for a silicone oil as continuous phase for three different  $w_d$ .



**FIG. 12.** The frequency of droplet generation (*f*) is mapped against the  $Ca_c$  for different  $w_c$ ,  $\lambda$ , and  $\phi$ . The experiments use hexadecane and silicone oil as continuous phase fluids.



**FIG. 13.** The frequency of droplet formation (*f*) is plotted against the  $Ca_c$  for various  $w_d$ ,  $\lambda$ , and  $\phi$  values.

width and the frequency of the droplet generation is observed to decrease. Experiments are conducted for silicone oil as continuous phase fluid and the results for different  $w_d$  are shown in Fig. 13.

A scaling model has been developed in the present study which can quantify the effects of geometrical variations and flow properties. The model developed in this study has been validated for the channels with dimensions greater than or equal to  $250 \,\mu$ m. However, for the microchannels with length scales of order 10 to  $500 \,\mu$ m, the dominant forces acting on the droplet's interface are the same. Hence, it can be considered that the model presented in this study is applicable for microchannels of length scales in  $O(20 \,\mu$ m). Various researchers<sup>17,38,42,45</sup> conducted their studies using microchannels with dimensions ranging from 20 to  $100 \,\mu$ m. They had used the same forces outlined in the current work for the analysis and development of the model. However, a comprehensive experimental study will be necessary to validate the present model for droplet generation inside the microchannels of  $O(20 \,\mu$ m).

#### V. CONCLUSIONS

In the present study, the investigation comprises a parametric analysis of the droplet size and frequency of droplet production for varying channel widths  $w_c$  and  $w_d$ . Though previous studies considered various channel parameters for predicting the droplet size, the physics behind the dynamics remained unclear. A theoretical analysis was carried out by taking into account Newtonian fluids without adding surfactants to either phase of the investigation. The model predicts the droplet size very well in both squeezing and dripping regimes for distinct  $w_c$  and  $w_d$ . The proposed mathematical model is validated with a large set of in-house experimental results that are consistent for different channel widths. In cases of varying  $w_c$ , the results lie parallel to each other when we take  $L/w_c$  as non-dimensional droplet length. However, the results collapse to a single curve when  $L/w_d$  is taken as non-dimensional droplet length. Reverse phenomena occurred when we vary dispersed channel width ( $w_d$ ). However, the conducted experiments are for channels having rectangular cross section only. The variation of frequency is presented in the current work at a wide range for varying  $w_c$ ,  $\phi$ , and  $\lambda$ . Also, the effect of different  $w_c$  on  $w_g$ , and  $t_{PN}$  are investigated thoroughly. The results show that both  $w_g$  and  $t_{PN}$  increase with an increment in  $w_c$  from 250 to 440  $\mu$ m. The significance of the scaling model is that it assists in the geometry-based design of microchannels. Our experimental evidence proves its applicability for the manipulation of droplets within a T-junction for varying channel widths. While the current model is valid for various flow rate ratios, channel width ratios, and viscosity ratios, it has not been verified for shallow channels.

#### SUPPLEMENTARY MATERIAL

See the supplementary material for: The abbreviations of each variable are given in the nomenclature. Figure S1 shows the plot of  $w_g$  for  $w_c$ = 250, 350, and 440  $\mu$ m, respectively. Corresponding experimental images are shown in Fig. S2. Figure S3 shows the plot for the frequency with respect to  $w_c$  for different  $Ca_c$ . Figures S4 and S5 depict the relationship between non-dimensional droplet length  $(L/w_d)$  and aspect ratio  $(h/w_c)$  for silicone and hexadecane oil as continuous phases, respectively.

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### AUTHOR DECLARATIONS

#### **Conflict of Interest**

The authors have no conflicts to disclose.

#### **Author Contributions**

Santosh Kumar Jena: Conceptualization (lead); Investigation (lead); Methodology (lead). Tushar Srivastava: Investigation (supporting); Methodology (supporting). Supreet Singh Bahga: Funding acquisition (equal); Methodology (equal). Sasidhar Kondaraju: Funding acquisition (equal); Investigation (equal); Methodology (equal); Supervision (equal); Writing – review & editing (equal).

#### DATA AVAILABILITY

The data that support the findings of this study are available from the corresponding author upon reasonable request.

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